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Preparation and Characterization of TiO₂-SiO₂ Bioceramic Coating on Ti Alloy via Electrochemical Anodization and Its Effect on Corrosion Resistance

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ABSTRACT

Purpose: The present study was carried out to study the effect of changing the anodization process parameters and investigate the corrosion resistance of the ceramic coating that will be formed on the CP-Ti by anodization method. **Materials and Methods:** CP-Ti samples of (10mm×10mm×2mm) were used for fabrication of bioceramic coating through anodization process with different parameters using potassium silicate as an electrolyte solution. The samples were characterized using XRD, AT-FTIR. The surface roughness was measured using ESEM and the surface topography was evaluated by SEM. Tafel polarization measurement and electrochemical impedance spectroscopy were used to detect the change in the corrosion resistance after anodization. **Results:** XRD revealed that the anodized coated samples showed well defined peaks at 2θ of Ti and TiO₂ and shallow peaks of SiO₂. AT-FTIR showed stretching bands of titania and silica. Regarding the surface roughness results, the anodized coated samples at the optimum conditions had the lowest Ra values while the uncoated (control) group had the highest Ra value. On comparing the results of the surface morphology, the best evenly distributed ceramic coat was formed at the optimum conditions where (the applied voltage =50v, the electrolyte concentration =3% and process duration=60min). The corrosion resistance of the anodized coated samples at the optimum conditions was markedly increased more than that of the uncoated CP-Ti samples. **Conclusions:** The optimum conditions of the anodization process to get a uniform anodized coating can be achieved when; the applied voltage is 50v, the electrolyte concentration is 3% and the process duration in 60min. Moreover, formation of a bioceramic coating has been shown to be a useful method for improving the corrosion resistance.

KEYWORDS

Anodization;

CP-Ti implant; Corrosion

Resistance;

Surface Morphology

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INTRODUCTION

For long time ago, dentists have been working to restore missing teeth with suitable materials. Dental implants are like screws that act as replacements for the anchorage of the missing natural tooth and becoming familiar in the recent day dental procedures⁽¹⁾. Not only the Ti-CP but also some alloys like binary and tertiary Ti alloys were in use. Regarding the recent reviews, it was concluded that most of the binary Ti alloys with alloying <20% elements of Zr, In, Ag, Cu, Au, Pd, Nb, Mn, Cr, Mo, Sn and Co have good impact as implant materials, as they have good mechanical properties⁽²⁾. Ti is commonly used as an implant material for its good biological acceptance, ability of bonding with osteoblasts and its acceptable biocompatibility. The spontaneous passive layer formed on the surface is almost reliable and can isolate the bulk Ti material from its environment. Therefore, it could resist the corrosion. Unfortunately, this oxide layer is very tiny and can be destroyed. Hence, various efforts have been done to preserve TiO coating⁽³⁾.

In an effort to improve corrosion resistance of the dental implant, the chemical structure and morphology of the implant surface need to be changed. Implant surface treatments have the opportunity of enhancing cell adhesion, cell growth, and bone formation which markedly improve the osseogenesis process⁽⁴⁾. There are different methods for modifying surface roughness or applying osteoconductive layers on titanium implants as titanium plasma-spraying, grit-blasting, acid-etching, anodization or calcium phosphate coatings, and their subsequent surface morphology and characteristics have proven clinical efficiency (>95% over 5 years)⁽⁵⁾.

From all these forementioned methods, anodization is of higher quality and sheep method which can provide controlled nanostructures on Ti surface. As many researches have shown that the osteoblasts are habituated to a nano-scale environment more than to a micro-scale environment.

The other methods are of more cost and may not provide both a thicker layer and acceptable cell adsorption^(6,7). It was claimed that anodic oxidation is a new technique in the biomedical field, a suitable method for making porous bioceramic films on surfaces of titanium. Moreover, it was stated that the benefits of these coating films is the higher cell adhesion, as the film formation includes oxidation the substructure^(8,9).

Scientists have tested ceramic oxides like Ti, Si, Nb, r mixed oxides and they have found that the oxides when formed on the metallic implant surface, provide an encouraging response to HA growth in vitro, osteoblast adhesion and proliferation in vivo and they also increased the wear and corrosion impedance of the dental implant⁽¹⁰⁾. Ti nano structures have a great importance in the medical field due to their special properties, expressed in the high repassivation rate, equivalent mechanical properties, increased surface area, and enhanced cell proliferation, adhesion and mineralization. However there is a deficiency in researches that could give exact knowledge about the main parameters and experimental variables needed to produce this such optimized structure⁽¹¹⁾.

A previous study incorporated the SiO₂ with titania nanotubes and they found that they are efficient in apatite nucleation while soaked in simulating body fluid. Also, it was claimed that Si is essential in bone formation with Ca and P⁽¹²⁾. Many scientists claimed that Si-containing bio-ceramics can help in the formation of apatite crystals. Therefore, it is very effective to add Si into the oxide film^(12,13). Convenient anodization parameters such as applied voltages, electrolyte concentration and different temperatures can equilibrate the growth and dissociation of the micro-nano surface structure⁽¹⁴⁾.

It was reported that the thickness of TiO₂ formed layer is mainly dependent on the voltage applied, which results to the believe that the TiO₂ layer has a high electrical resistivity. The morphological

structure can be handled by changing the factors of the process, which are the voltage applied, electrolyte type, and duration of the process⁽¹⁵⁾. It is known that HA form and grow on anatase phase of TiO₂ relatively more than on rutile one. Therefore, heat treatment of TiO₂ nanotubes at 350 °C is required for changing the amorphous to crystalline structure with anatase phase⁽¹⁶⁾. It was also found that anatase crystallites formed inside the tube walls and changed totally to rutile at about 600 °C in dry environments and 570 °C in humid argon⁽¹⁷⁾.

Another study evaluated the surface modifications of titanium implants. The surface topography was examined using SEM. They demonstrated that the main differences in the surface properties were mainly depending on the type of surface treatment utilized. They concluded that anodization process for Ti-Unite implants provides microporous surface (pore size: 0.5-3.0microm), moreover, it changes the surface chemistry due to incorporating the ions of the used electrolyte⁽¹⁸⁾.

The corrosion resistance of Ti alloy was determined. Anodization process for surface alteration was used. The surface topography, chemical structure and the formed phases of the CP-Ti and surface treated Ti-6Al-4V alloy were inspected using (SEM), (EDX), (XPS) and X-ray diffraction (XRD). They found that the anodization process produced porous coating. The bioactivity study in (SBF) solution and with human bone marrow stromal cells (MSCs) revealed that after anodizing at 140 V and after alkali treatment the Ti-6Al-4V alloy shows osteoinductive behavior. The corrosion resistance evaluation showed that application of the anodizing process of the Ti-6Al-4V alloy apparently increased its corrosion resistance in Ringer solution⁽¹⁹⁾.

MATERIALS AND METHODS

CP-Ti foil (Sigma Aldrich-USA), Etching solution (mixture of HF+NHO₃+H₂O), Ethanol, Potassium Silicate (Loba Chemie-India), Ringers' solution (ADWIA-Egypt) were used in the present study.

Samples' preparation:

The CP-Ti foil was cut into samples of (1cm 1cm 0.2cm) using wire cut machine. The samples were polished before starting the anodization process by sand paper disks up to 1200 grit. After that, the samples were etched for 30 seconds using HF+NHO₃+H₂O with the ratio of 1:4:5 then, washed using deionized water and ethanol alternatively for five minutes and dried with air dryer.

Sample's grouping:

Regarding to the anodization process, three parameters were studied; (applied voltage, electrolyte concentration and process duration). A total of (90) samples were prepared for the laboratory study. Each parameter was divided into three groups so that the total number of the groups was nine groups in addition to a control group (n=9).

Formation of bioceramic coating:

The anodization process was done exploiting two-electrode joined with a direct current power provider. CP-Ti was used as anode having the surface area of 1cm² and platinum basket was used as cathode in a temperature controlled set up. To investigate the effect of changing the anodization parameters on the properties of anodic coating, the process was done in different i) applied voltage (40 v – 60 v) ii) concentration of K₂SiO₃ (2% - 4%) and process duration (30 min – 90min). Following anodic oxidation, the samples were washed with deionized water and annealing was done to get crystallized phases (oxygen crystallization) at 350 °C for 5 hours.

Characterization of the formed coat:

The surface chemistry of the formed ceramic coat was investigated using AT-FTIR (400 Perkin Elmer infrared spectrometer), the new formed phases on the CP-Ti surface was confirmed using XRD (PHILIPS-binary scan), surface roughness was detected by ESEM (Quanta 200- company FEI - Netherlands) and surface morphology was examined by SEM Quanta 250 FEG-Netherlands).

Corrosion studies

The corrosion studies of the different CP-Ti samples surfaces' before and after anodization process were carried out using Electrochemical workstation- metrohm autolab (NOVA 1.11) by the use of ringer's solution. A three electrode build up was established for corrosion testing, where Platinum is used as counter electrode, Ag/AgCl was used as reference electrode and the anodized coated sample was the working electrode for both Tafel and impedance measurements. The surface area of working electrode was maintained at 0.38 cm². Tafel measurements were performed by applying potential in the range of +2 V to -2 V with a scan rate of 0.001 mV/s. The impedance measurements were done by using a sinusoidal wave of 10 mV to the working electrode at a frequency range of 0.1 MHz – 10 MHz.

Statistical analysis

The differences between Control group and the groups in each parameter were tested. ANOVA test was used to determine whether the differences are significant or not. As the differences were significant, the Post Hoc test (Tukey's method for multiple comparisons) was done to confirm that the variation returns to each group. The statistical analysis was done with IBM SPSS Statistics Version 20 for Windows.

RESULTS

Results of Anodization Process:

The color of the samples changed from the normal silvery white of the CP-Ti to different other colors by proceeding in the anodization parameters' variables. Regarding the applied voltage; the color changed to (yellow, brown, blue). Regarding the electrolyte concentration; the color changed to (orange, brown, pink). Regarding the process duration; the color changed to (fuchsia, brown, purple).

Surface characterization:

Results of XRD analysis:

Regarding the control group; Sharp and well defined peaks corresponded to Ti and TiO₂ phases were found. Regarding the anodization parameters (V, C and D): sharp and well defined peaks of corresponded to Ti and TiO₂ phases. A new peak of the SiO₂ phase was represented by a shallow peak (figures 1 and 2).

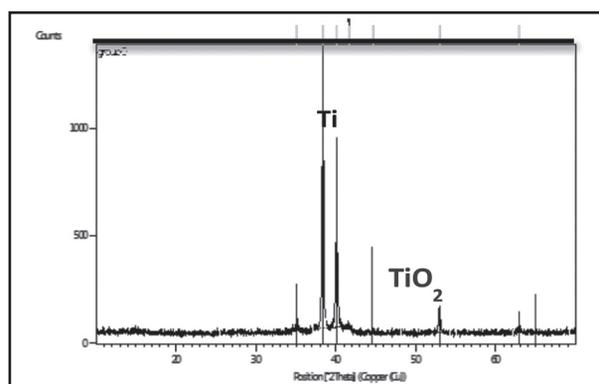


Figure (1) XRD pattern of the control group

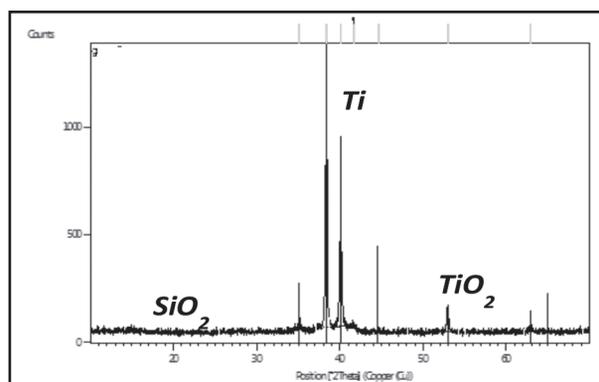


Figure (2): XRD pattern of the anodized coated showing the Ti and TiO₂ peaks samples showing the Ti, TiO₂ and SiO₂ peaks

Crystal shape and Size of the Control group and the Anodized coated groups:

Table (1) shows the crystal size and shape of the formed phases. Ti phase was varying from hexagonal to cubic crystalline structure, TiO₂ phase was in the form of tetragonal crystalline structure

Table (1): The crystal size and shape of the formed phases:

| Crystal Size(nm) \ Goup | Control | Applied voltage (V) | | | Electrolyte concentration (C) | | | Process duration (D) | | |
|----------------------------------|-----------|---------------------|------------|----------|-------------------------------|------------|-----------|----------------------|------------|-----------|
| | | V=40 | V=50 | V=60 | C=2% | C=3% | C=4% | D=30m | D=60m | D=90m |
| CP-Ti Hexagonal & cubic | 14-126 nm | 27-76 nm | 55- 380 nm | 21-32 nm | 39-2 nm | 57- 380 nm | 32-110 nm | 32-95 nm | 55- 370 nm | 19-120 nm |
| TiO ₂ Tetragonal | ----- | 22-42 nm | 37- 312 nm | 19-90 nm | 20-38 nm | 30- 323 nm | 30-122 nm | 22-30nm | 36- 310 nm | 19-78 nm |
| SiO ₂ Rhombohedral | ----- | 29-37 nm | 19-320 nm | 7-20 nm | 20-100 nm | 19-320 nm | 20-130 nm | 11-15 nm | 15-317 nm | 19-70 nm |

and the SiO₂ phase was in the form of rhombohedral crystalline structure. Regarding to the crystalline size; there was a change of the crystal size through the variables of all the anodization parameters in the same trend.

Results of Attenuated Reflectance Fourier Transform Infrared (AT-FTIR):

Frequencies of the absorption bands of AT-FTIR spectra of control and anodized samples with different anodization parameters (V, C, D) were recorded by diffused reflection from 4000 to 400 cm⁻¹ (figures 3 and 4).

Surface Roughness Measurement (Ra):

Table (2) and Figure (5) show the mean and standard deviation (SD) of surface roughness (Ra) in nm of the control group and the anodized coated groups. Regarding the applied voltage parameter; the highest surface roughness was for group (V=60v) and the lowest surface roughness was for group (V=50v) in comparison with the control group. Regarding the electrolyte concentration; there was no statistically marked difference between the groups (C=2%, C=3%). Regarding the process duration; the highest surface roughness was for group (D=90min) while, the lowest value was for group (D=60min).

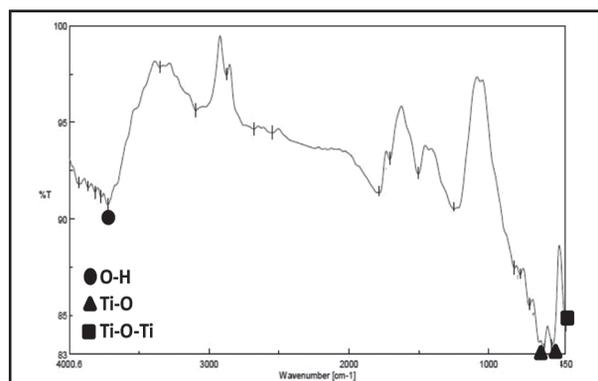


Figure (3): AT-FTIR spectrum of the control group showing the stretching bands of O-H, Ti-O, Ti-O-Ti

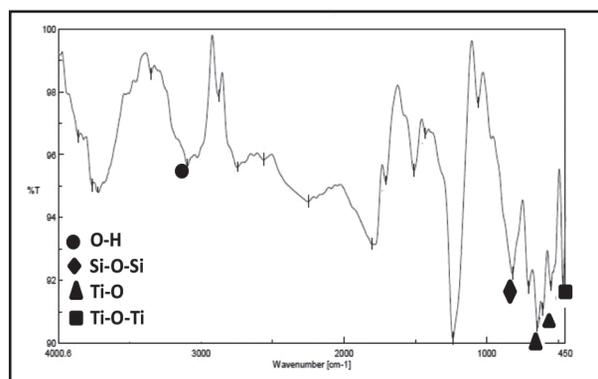
Figure (4): AT-FTIR spectrum of the anodized coated samples showing the stretching bands of O-H, Ti-O, Ti-O-Ti and SiO₂

Table (2): The mean and standard deviation (SD) of surface Roughness (Ra) in nm of the control and the anodized coated groups:

| Group | Control | Voltage (V) | | | Concentration (C) | | | Duration (D) | | |
|----------|-------------------|-------------------|-------------------|--------------------|-------------------|-------------------|--------------------|-------------------|-------------------|-------------------|
| | | V=40v | V=50v | V=60v | C=2% | C=3% | C=4% | D=30min | D=60min | D=90min |
| Mean | 2.84 ^e | 7.44 ^b | 4.63 ^d | 15.31 ^a | 4.40 ^d | 4.50 ^d | 13.05 ^a | 5.58 ^c | 4.75 ^d | 7.04 ^b |
| S.D | 0.257 | 0.942 | 1.587 | 1.217 | 0.399 | 1.211 | 2.765 | 2.167 | 1.530 | 1.206 |
| P- value | P ≤0.000* | P ≤0.000* | | | P ≤0.000* | | | P ≤0.000* | | |

*: Significant at $P \leq 0.05$, Different letters in the same row are statistically significantly different according to Tukey's test

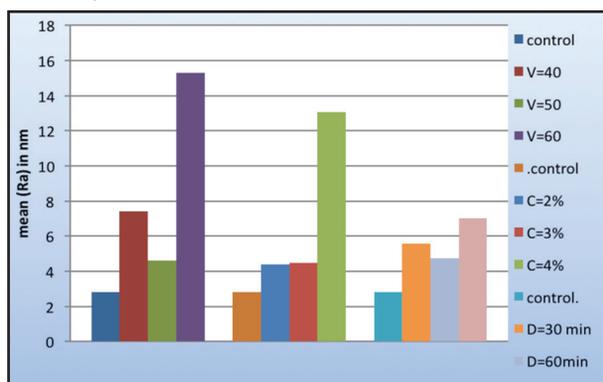


Figure (5): A bar chart representing the mean Ra values in (nm) of control group and the anodized coated groups with different anodization parameters.

Topographical 3D Images of the control group and the anodized coated groups using ESEM:

In comparison with the control group (figure 6-a), the surface roughness of the anodized coated samples increased at the beginning of the process (figure 6-b), then, by preceding in the process the surface roughness decreased showing shallow valleys and slightly broad elevated projections (figure 6-c). Finally, the surface roughness increased once again revealing deep valleys with prominent sharpened and pointed peaks (Figure 6-d).

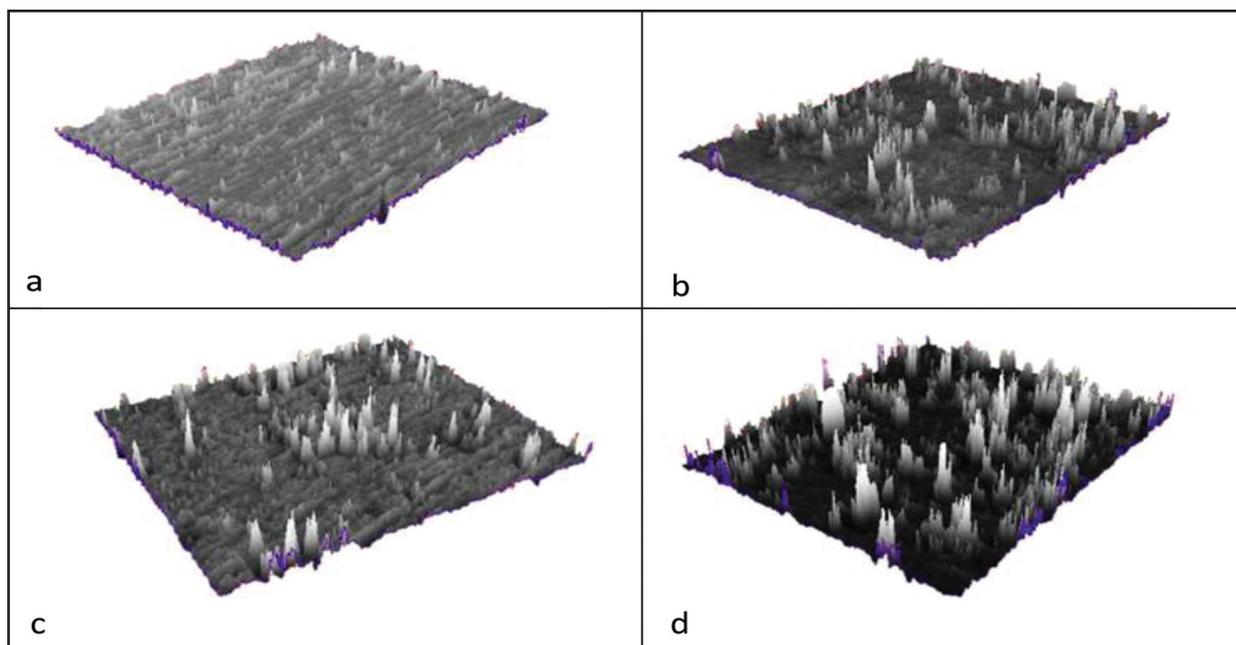


Figure (6): 3D Surface roughness of the control group and the anodized coated groups at different anodization parameters' variables

Surface morphology of the control group and the anodized coated groups using SEM:

A representative Scanning Electron Micrographs were selected for the investigated groups. Figure (7) shows the control group with normal appearance of the CP-Ti surface after polishing and the anodized coated samples where few crystals of SiO₂ were deposited on the sample surface and some islands of TiO₂ were formed (figure 7-b). By proceeding in the process where (V=50, C=3%, D=60) enlargement of the silica crystals took place and fusion of the titania islands were found to form a uniform layer with well distribution of its constituents (figure 7-c). Finally, at the highest variables cracks were

developed and micro porosities were found in the formed coat (figure 7-d).

Corrosion studies

Tafel polarization technique:

The parameters obtained from the potentiodynamic curves; (Tafel polarization) were displayed in (Table 4). The Tafel polarization curves showed that the resistance of anodized coated samples improved by proceeding in the anodization parameters; (applied voltage, electrolyte concentration and process time) which in turn led to marked decrease in the corrosion rate.

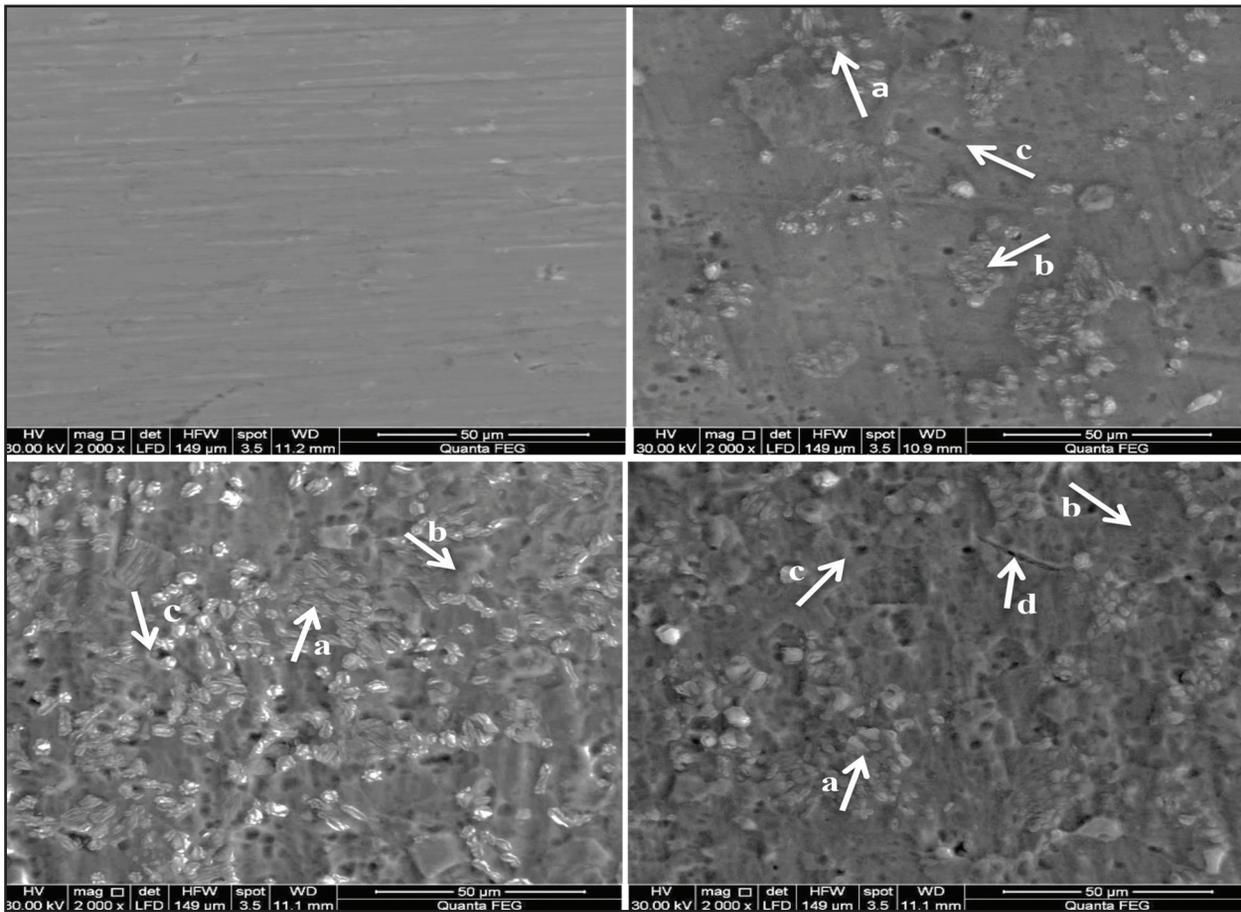


Figure (7): SE micrographs of the control group and the anodized coated groups where: The (a) arrow pointed to the silica crystals, the (b) arrow pointed to the titania islands, the (c) arrow pointed to the porosities, the (d) arrow pointed to the developed cracks.

Table (3): Corrosion resistance and Corrosion rate the control group and the anodized coated groups regarding different anodizaion Parameters (V, C, D):

| | Control | Applied voltage | | | Electrolyte concentration | | | Process duration | | |
|---------------------------|-----------|-----------------|------------|-------------|---------------------------|-------------|-------------|------------------|-------------|-------------|
| | | V=40 | V=50 | V= 60 | C=2% | C=3% | C=4% | D=30min | D=60min | D=90min |
| Corrosion resistance (kΩ) | 127.570 Ω | =89.320 kΩ | 461.380 kΩ | =171.070 kΩ | 122.690 kΩ | =478.550 kΩ | =145.020 kΩ | =235.160 kΩ | =492.310 kΩ | =444.500 kΩ |
| Corrosion rate (mm/year) | 0.10774 | 0.01341 | 0.00092 | 0.02366 | 0.04055 | 0.00108 | 0.00415 | 0.01124 | 0.00130 | 0.00491 |

Electrochemical Impedance Spectroscopy (EIS):

The equivalent circuit of the control group and the anodized coated group of the highest corrosion resistance and the lowest corrosion rate (optimum conditions; V=40v, C=3%, D=60min.) was demonstrated in (table 4) based on EIS fitted curves. Like in the Tafel data, EIS study also revealed that the selected anodized coated CP-Ti group had higher corrosion resistance compared to that of the control group.

Table (4): The Corrosion Resistance, Electrical Double Layer Capacitance and Solution Resistance Regarding the Control Group and the Anodized Coated Group:

| Group Parameter | Control group | Anodized coated group |
|--|---------------|-----------------------|
| Corrosion resistance (R_{ct}) | 112 KΩ | 247.7 KΩ |
| Electrical double layer capacitance (C_{dl}) | 18.1μMho | 11.5 μMho |
| Solution resistance (R_s) | 142 Ω | 205 Ω |

DISCUSSION

Generally, the long-term service of dental implants is acceptable. However, the failure of dental implants still occurs in a small quantity of patients. There are few researches studying the failed Ti dental implants due to rusting and erosion and its effect on

anchorage and biological aspects⁽²³⁾. Patients remain a great challenge in dental implantology and prompt the need for bioactive surface modifications that accelerate osseointegration after implant insertion. In addition, the aim of designing new bioactive surface properties is to accelerate osseointegration for more convenient, early loading protocols. The main task of biomedical studies on surface alterations is to facilitate early osseointegration and to secure longevity of bone-to-implant contact without subsequent bone loss at the interface⁽²⁴⁾. Therefore this work was conducted to modify the surface of the dental implant and evaluate the effect of this surface modification on improving its corrosion resistance.

In the current study; CP-Ti foil was used as it is considered as good biomedical *material*. Precision and longevity of these implants are guaranteed by the combined effect of high fatigue strength, good corrosion resistance, biocompatibility and free of toxic elements compared with other older materials⁽²⁵⁾. Anodization process was selected as it is the most easy and inexpensive reliable method to fabricate (nano-micro) porous oxide layer without adding any foreign materials to the samples⁽²⁶⁾. Moreover, TiO₂-SiO₂ bioceramic coating fabrication was selected in this study as a surface modification of the CP-Ti dental implant because it has synergistic action on biocompatibility and corrosion resistance, ideal combination of potential bioactivity on the surface with desirable mechanical properties and osteoblastic cell adhesion.

A mixture of (HF+HNO₃+H₂O) was used as an etching solution in the present study. The use of HF as etching solution might allow the formation of soluble TiF₄ species due to high reactivity of Ti to fluorine incorporated fluorides that are favorable to osseointegration of dental implants. HNO₃ make the etching solution more stable, allows the elimination of H₂ gas and accelerates the etching rate⁽²⁷⁾. Cleaning after etching and before starting the electrochemical anodization process is essential because of the high chemical reactivity of titanium which can lead to its contamination or embrittlement, and can increase its susceptibility to stress corrosion⁽¹⁰⁾.

Potassium silicate was used (as a silica source) as an electrolyte in the anodization process as it is known that the aqueous *silicate* solutions support precipitating and forming mixed silica nanoparticles. In addition, silica coating nanoparticles solve the problem of peri-implantitis as it has antibacterial effect and in turn it improves the osteointegration and bone formation. Furthermore, it was claimed that silica coating improves the corrosion resistance of the anodized Ti surface⁽²⁸⁾. Oxygen crystallization of the anodized coated samples was done in the furnace to be sure that all the newly formed phases were of crystalline structure. Furnace or air cooling is preferred as oil or water quenching can promote non-uniform cooling, which can induce residual stresses⁽²⁹⁾.

Characterization of the ceramic coating was done using the samples without being grinded as only the formed phases on the surface of the samples were to be detected using (XRD). In the present study, (figures 1, 2) the presence of sharp and strong intense peaks of TiO₂ with tetragonal crystal structure, in addition to a weak and not well defined peak corresponds to silica in the form of rhombohedral crystals in all the anodized coated groups. This may be attributed to two reasons; the super imposition of the titania peak over that of the silica peak and due to the small amount of the silica incorporated in the coat compared to that of titania.

Regarding Surface roughness; the surface roughness linearly decreased up to the optimum conditions (V=50, C=3%, D=60) then, increased again owing to the fact that the higher voltage afforded a higher chance for the ions which needed for anodic growth and it was possible to increase the presence of SiO₂ into the oxide coating hence, decreases the surface roughness. Moreover, increased presence and inward diffusion of the oxygen ions (O²⁻) towards the Ti/oxide interface in the bath increased that interacted with the Ti⁴⁺ ions that are travelled out of the Ti surface. So, the oxide layer covered the whole surface of the sample. Furthermore, increased addition of SiO₂ into the oxide film leads to the stabilization of the coating. The fabrication rate of the coat is in direct relation with the thickness of the oxide layer produced per time. Therefore, when the process duration is increased, the interaction between the titanium electrode and oxide ions was taking place for a longer duration, which might increase the thickness of the anodized coating. This finding was supported by the results of the SEM that showed enlargement of the crystals to form islands making the surface more smooth (figure 7-c)^(30,31). However, increasing the anodization parameter variables led to increase in surface roughness. This may be caused by the amount of heat liberated that couldn't be completely and effectively dissipated from the anodic titanium surface (although with the presence of the electrolytic cell in a water bath of controlled temperature) which as a consequence, increased the dissociation thereby strongly leading to the breakdown of the oxide coat. Also, with higher applied voltage, dissolution of the ions increased leading to production of more quantities of potassium ions to form potassium hydroxide, which in turn synergize the pH of the electrolyte which results in the dissolution of the coating (table 2, figure 6).

Regarding surface morphology; at the optimum conditions (V=50, C=3%, D=60), a smooth and uniform distributed oxide coat with normal

arrangement of dome like structure was formed. This may be due to the addition of SiO_2 which decreased the structural defects of the coating. With higher electrolyte concentration ($C=4\%$) some micro cracks appeared on the formed film which might be the result of internal stress developing in the oxide film on the Ti surface due to the micro cracks developed and the volume expansion. However, the incorporation of SiO_2 into the oxide film is high at this condition due to the diffusion through the cracks and the porosity. The results of the SEM of this study were in accordance with that of another study which claimed that the cracks in the coatings might be caused by the production of O_2 bubbles during anodization⁽³¹⁾ (figure 7).

Regarding Corrosion results; Tafel polarization results showed that the best corrosion resistance and the lowest corrosion rate was gained at the anodization parameters ($V=50$, $C=3\%$, $D=60$). This may be due to the good quality of the formed coating obtained at the optimized conditions. As the imperfections are very little in the formed coat at optimum condition, the corrosive media can't diffuse through the formed coat easily. Therefore, the results proved that the corrosion resistance of the coat was depending on its morphology and the properties of the oxide film (table 3). Moreover, the electrochemical impedance results showed that the formed oxide layer on the samples' surface had a double effect on the corrosion process of Ti; it decreased the rate of charge transfer process and decreased the penetration across the surface layer⁽³²⁾. This may be attributed to the fact that the presence of SiO_2 along with TiO_2 which formed a protective shield thus decreased the deterioration of the coating compounds owing to its impeding property. These results were in accordance with the work that done in a previous study which studied the effect of the similar parameters and concluded that the corrosion resistance was increased linearly as the parameters increased⁽³³⁾ (table 4).

CONCLUSIONS

Within the limitations of the current study the following could be concluded:

1. Anodic oxidation is an effective method for preparing bioactive titanium metal as an implant material.
2. The surface roughness could be tailor made by changing the parameters of the anodization process.
3. Applied voltage, electrolyte concentrations and process duration, clearly influenced the morphological and topographical features, as well as the chemical composition of the anodized coated layer.
4. The optimum conditions of the anodization process to get a uniform, dense and compact anodized coating can be achieved when; the applied voltage is 50v, the electrolyte concentration is 3% and the process duration in 60min.
5. Formation of a bioceramic coating has been shown to be a useful method for improving the corrosion resistance.

REFERENCES

1. Krishna A R, Ginjupalli K, Upadhy N, Shammam M, Krishna R R, Sekhar R. Surface Roughness of Implants: A Review. Trends Biomater. Arti. Organs.2011; 25:112-8.
2. Liu X, Chen S, James K H, Matinlinna T J P. Binary titanium alloys as dental implant materials—a review. Regen Biomaterials. 2017; 4: 315–23.
3. Pavón J, Galvis O, Echeverría F, Castaño, M. Echeverry, S. Robledo et al. Anodic oxidation of titanium for implants and prosthesis: processing, characterization and potential improvement of osteointegration. V Latin American Congress on Biomed Eng.2013; 33: 176–9.
4. Yuan L J, Edmond H N P, Zheng L W, Ma L, Dora L W K, Cheung L K. Effects of Calcium Phosphate Nanocrystals on Osseointegration of Titanium Implant in Irradiated Bone. Biomed Res. Inter. 2015; 78:1- 6.
5. Guéhennec L L, Soueidan A, Layrolle P, Amouriq Y. Surface treatments of titanium dental implants for rapid osseointegration. Dent Mat. 2007; 23: 844–54.

6. Portan D V, Kroustalli A A, Deligianni D D, Papanicolaou G C. The biocompatibility between TiO₂ nanotubes layer and human osteoblasts, *J. Biomed. Mat. Res.* 2012; 100: 2546–53.
7. Minagar S, Wang J, Berndt C C, Ivanova E P, Wen C. Cell response of anodized nanotubes on titanium and titanium alloys—a review, *J. Biomed. Mat. Res.* 2013; 101: 2726–39.
8. Krupa D, Baszkiewicz J, Zdunek J, Smolik J, Slomka Z, Sobczak J W. Characterization of the surface layers formed on titanium by plasma electrolytic oxidation. *Surf Coat Tech.* 2010; 205: 1743–9.
9. Curran J A, Clyne T W. The thermal conductivity of plasma electrolytic oxide coatings on aluminium and magnesium. *Surf Coat Tech.* 2005; 199: 177–83.
10. Mumjitha M Raj V. Fabrication of TiO₂ - SiO₂ bioceramic coatings on ti alloy and its synergetic effect on biocompatibility and corrosion resistance; *J Mech Behav Biomed Mat.* 2015; 46: 205-21.
11. Khudhair D, Bhatti A, Amani Hamedani H, Garmestani H, Hodgson P, Nahavandi S. et al. Anodization parameters influencing the morphology and electrical properties of TiO₂ nanotubes for living cell interfacing and investigations. *Mat Sci Eng.* 2016; 59: 1125–42.
12. Fahim N F, Morks M F, and Sekino T. Electrochemical synthesis of silica-doped high aspect-ratio titania nanotubes as nanobioceramics for implant applications, *Electrochim. Acta* 2009; 54: 3255–69.
13. Carlos D, Borrajo J P, Serra J, Gonzalez P, Leon B. Behaviour of MG-63 osteoblast-like cells on wood-based biomorphic SiC ceramics coated with bioactive glass, *J. Mater. Sci: Mater. Med.* 2006; 17: 523–29.
14. Lianga J, Liua K, Wanga D, Lia H, Lib P, Lib S et al. Facile fabrication of superhydrophilic/superhydrophobic surface on titanium substrate by single-step anodization and fluorination. *App Surf Sci.* 2015; 338: 126–36.
15. Takadom J. *Nanomaterials and Surface Engineering*, John Wiley with Sons. 2013; e-book: 1-30.
16. Xiao X, Liu R, Rongfang L. Synthesis and bioactivity of highly ordered TiO₂ nanotube arrays. *Appl. Surf. Sci.* 2008; 255: 365–7.
17. Oomman K V, Gong D, Paulose M, Craig A. Grimes E C D. Crystallization and high-temperature structural stability of titanium oxide nanotube arrays. *J Dent Res.* 2011; 18: 156-65.
18. Kang B S, Sul Y T, Oh S J, Lee H J, Albrektsson T. XPS, AES and SEM analysis of recent dental implants. *Acta Biomater.* 2009; 5: 2222–9.
19. Krzakala A, Słuzalska K, Widziołek M, Szade J, Winiarski A, Dercz G. et al. Characterization of bioactive films on Ti–6Al–4V alloy. *Electrochimica Acta.* 2013; 104: 425–38.
20. Robert J O, David R J. *Organic Chemistry Study Guide. Key Concepts, Problems and Solutions* 2015; 1st Edition: 614.
21. Badr N A, Shoreibah E A, Khafagi M G, Motawea I T, Mahmoud F. The exploitation of implants' surface as drug delivery device (an in vitro study). Thesis. 2012
22. Yang Y, Jiming B, Chong W Michael J A. Sub-bandgap luminescence centers in silicon created by self-ion implantation and thermal annealing. *J Appl Phys.* 2010; 107: 123-9.
23. Revathi A, Alba D B, Anna I M, Caroline R C, Manivasagam G. Degradation mechanisms and future challenges of titanium and its alloys for dental implant applications in oral environment. *Mater Sci Eng.* 2017; 76: 1354-68.
24. Gómezde D R, Mangde R M, Romero Pérez M J, Cutando A, Valverde L A. Indications and contraindications of dental implants in medically compromised patients: update. *Medicina Oral, Patología Oral y Cirugía Bucal.* 2014; 19: 483–9.
25. Polyakov A V, Semenova I P, Valiev R Z. High fatigue strength and enhanced biocompatibility of UFG CP Ti for medical innovative applications. *IOP Conference Series: Mater Sci Eng.* 2014; 63: 121-3.
26. Chellappa M, Vijayalakshmi U. Effect of silica fiber on the mechanical and chemical behavior of alumina-based ceramic core material. *J Asi Cer Soc.* 2017; 5: 326-33.
27. Yamamoto D, Kawai I, Kuroda K, Ryoichi I, Masazumi O, Azusa S. Osteoconductivity of Anodized Titanium with Controlled Micron-Level Surface Roughness. *mater trans.* 2011; 52: 8.
28. Marcus J, Herbert P J, Florian D, Alfons F, Hedda L. Antimicrobial and Osseointegration Properties of Nanostructured Titanium Orthopaedic Implants. *Materials.* 2017; 10: 130-2.
29. Matthew J, Donachie J. Heat Treating Titanium And Its Alloys *Heat. Treat Prog mag.* 2001; 1: 49-50.
30. Voon C H, Derman M N. Effect of Electrolyte Concentration on the Growth of Porous Anodic Aluminium Oxide (AAO) on Al-Mn Alloys. *Adv Mater Res.* 2014; 626: 610-14.

31. Liang W, Jianhua L, Mei Y, Songmei L, Hongxing L, Mengqi Z. Effect of Anodization time on Morphology and Electrochemical Impedance of Andic Oxide Films on Titanium Alloy Int. J. Electrochem. Sci. 2014; 9: 5012 - 24.
32. Mumjitha M, Raj V. Electrochemical synthesis, structural features and photoelectrocatalytic activity of TiO₂-SiO₂ ceramic coatings on dye degradation. Mater Sci Eng. 2015; 198: 62-73.
33. HongBok C, HanSeung L, Mohamed A I, Warid M H. Evaluation of Electrochemical Impedance Properties of Anticorrosion Films by Arc Thermal Metal Spraying Method. Int. J. Electrochem. Sci. 2015; 10: 9775 – 89.